Design and Simulation Experiment Research of a New Jaw Movement Robot

Cong Ming, Du Jing, Liu Tongzhan, Wen Haiying, Xu Weiliang

Abstract—To achieve the high bio-imitability requirements, we propose a novel human jaw movement robot based on mechanical biomimetic principles. First, according to the biomechanical properties of mandibular muscles, such as unsymmetrical distribution, force with different direction and the joints in maxillary and mandible is non-coplanar, a robot that simulates the jaw movements is built based on the 6-PS parallel mechanism. Then, its inverse kinematics solution equation and Jacobian matrix are driven. Finally, experiment study of jaw movement on the platform of virtual prototype shows that the parallel mechanism can meet the demands, such as reality of mandibular movement trajectory and rationality of occlusal force.

Index Terms—jaw movement robot, parallel mechanism, kinematics analysis, simulation

I. INTRODUCTION

Human mandible system mainly consists of lower jaw, muscle and temporal mandibular joint. Performing complex periodic opening and closing movement relative to the maxillary in three-dimensional space, lower jaw is alternately driven by several opening and closing muscles [1]. Jaw muscles mainly include the masseter, temporalis, and pterygoid muscle, which present symmetric distribution [2]. In the physiological activities of the human body, jaw system assumes the responsibility of several essential physiological functions, like chewing food, expressing language and controlling expressions.

The research of the jaw movement robot which can simulate human mandible movement and reproduce human mandible force began in the 1990s [3]. In accordance with the application field of the jaw movement robots, they can be classified as follows: In dentistry, such as Alemzadeh etc. [4] developed a dental test simulator based on Stewart platform, which can be used for experiment of dental component material. Callegari etc. [5] propose a kind of 3-PUU parallel mechanism that can auxiliary dentist to perform dental disease pathology research in the mandible motion situation. The biological characteristics of human mandible system has not been considered in the two robots above, so they could not really reappear function and environment of the mandible movement; In food science, references [6]–[9] has made the unique contribution to the mastication robot. Among them, the mechanism, which the article [8] proposes, exists serious problems of the singular configuration so that it couldn’t achieve the required mandible movement and bite force during the process of food chewing; In biomechanics, there are Mark III mastication mechanism [10], JSN chin simulator [11]–[12], and mandible motion simulator [13] etc., which are mainly used to study the movement characteristics of the mandible system. In addition, Takanobu etc. [14] developed a rehabilitate robot aiming at mandible movement, and E. Flores etc. [15] propose a language physical therapy robot for the research of perception and comprehension function in the process of talking face to face.

Synthetically considering the biological characteristics of the mandible muscles, including asymmetry distribution, different direction of the force, and non-coplanar junction of the mandible bones, this paper designs a new jaw movement robot based on the mechanical bionic principle. In accordance with the characteristics of the new jaw movement robot, this paper combines with the analytical method, the kinematics simulation and experiment test to analyze and verify the feasibility of the structure design, the reliability of the movement trajectory and the rationality of the bite force.

II. DESIGN OF JAW MOVEMENT ROBOT

A. Design of the General Structure

The CAD model and sketch of jaw movement robot, including the end-effector (mandible mechanism) and six branched chains of the kinematic pairs are shown in Fig. 1 and Fig. 2. In the CAD model, the support and upper jaw of the structure are omitted to simplify the mandibular structure. The force from mechanism branched chains to mandible, whose point is located at the connection of jaw muscle, works in the direction of muscle action line. In the structure, spherical joint S and shifting pare P are used to simulate the muscle contact point and driving muscle, respectively. The position of the sliders is changed through motors to implement mandible space motion.
jaw bones coincide with the connection positions of the chain with upper and lower jaw mechanisms, and the length deduces the action points, which connect each branched feasibility requirements of the mechanism, this paper etc. Comprehensively considering the high bionic design and position of connection points, length, and cross sectional area measured the parameters of those muscles, including mandible driving muscles. J.H.Koolstra etc [16] has between both side muscles, the paper just shows the action points position of the left muscles’ resultant forces in the mandible coordinate, as shown in TABLE 1.

### III. Inverse Kinematics

In order to develop the robotic mechanism, a frame Oxyz (or static frame) and a frame Oxym (or mandible frame) are established based upon the human skull and mandible. The origin of the mandible frame which has a sagittal plane (x-z plane), a frontal plane (y-z plane), and a horizontal plane (x-y plane) is located at the symmetrical center of the mandibular molar. The position of the mandible frame relative to the static frame can be determined by homogenous transform \( b_R^O \) as follows:

\[
\begin{bmatrix}
  c\gamma c\beta -s\gamma c\alpha c\beta s\alpha + s\gamma s\beta s\alpha & s\gamma c\beta c\alpha -c\gamma s\beta s\alpha & b_O^z \\
s\gamma c\beta c\alpha + c\gamma s\beta s\alpha & c\gamma c\beta s\alpha -s\gamma s\beta c\alpha & b_O^y \\
-s\beta & c\beta s\alpha & b_O^x \\
0 & 0 & 1
\end{bmatrix}
\]

In which: \( c = \cos \), \( s = \sin \).

In which, \( ^bO_m = \{^bO_{mx},^bO_{my},^bO_{mz}\} \) is the origin of the Oxym with respect to Oxzy, and \((\alpha, \beta, \gamma)\) are roll-pitch-yaw rotational angles about the static frame’s x, y and z axes, respectively. The position and posture of the mandible mechanism change from the two group decision variables above.

The completed robot displays the following configuration for the initial position:

\[
\{^iO_{mx},^iO_{my},^iO_{mz}\} = \{0,0,100\}^T, \ (\alpha, \beta, \gamma) = \{0^\circ,0^\circ,0^\circ\}
\]

On one hand, vector \( \vec{B_iM_i} \) as shown in Fig. 3 can be found explicitly as follows:

\[
\vec{B_iM_i} = \vec{B_iO_i} + \vec{O_iO_m} + \vec{O_m}M_i
\]

\[
\vec{B_iM_i} = \begin{bmatrix} B_{ix} \\ B_{iy} \\ B_{iz} \end{bmatrix} + \begin{bmatrix} ^iO_{mx} \\ ^iO_{my} \\ ^iO_{mz} \end{bmatrix} = \begin{bmatrix} B_{ix} + ^iO_{mx} \\ B_{iy} + ^iO_{my} \\ B_{iz} + ^iO_{mz} \end{bmatrix}
\]

Where the first term \( \vec{B_iO_i} \) is determined by the location coordinates of Oxym on the static frame; the second term \( \vec{O_iO_m} \) is determined by the initial position and posture of the mandible; and the third term \( \vec{O_m}M_i \) is determined by the location of Mi on the mandible.

On the other hand, vector \( \vec{B_iM_i} \) can also be expressed by:

\[
\vec{B_iM_i} = \vec{B_iC_i} + \vec{C_iM_i}
\]

Rearranging (4) gives rise to:

\[
\vec{C_iM_i} = \vec{B_iM_i} - \vec{B_iC_i}
\]

Further squaring the norm of the above vector equation yields:

\[
\|\vec{C_iM_i}\|^2 = \|\vec{B_iM_i}\|^2 - 2 \vec{B_iM_i} \cdot \vec{B_iC_i} + \|\vec{B_iC_i}\|^2
\]

In which \( \|\vec{C_iM_i}\| = L_i (i = 1,2,\ldots,6) \) is the length of each bar, and \( \vec{B_iM_i} \) is calculated by (3). Letting

\[
\|\vec{B_iM_i}\|^2 = r_i^2
\]

### B. Design of the Mandible Driving Muscle Structure

The coordinates of the points connected the drivers and jaw bones coincide with the connection positions of the mandible driving muscles. J.H.Koolstra etc [16] has measured the parameters of those muscles, including position of connection points, length, and cross sectional area etc. Comprehensively considering the high bionic design and feasibility requirements of the mechanism, this paper deduces the action points, which connect each branched chain with upper and lower jaw mechanisms, and the length of each branched chain. Owing to the complete symmetry between both side muscles, the paper just shows the action
The vector direction of $\overrightarrow{BC}$ is $\tau = [0, 0, 1]^T$, so
$$\overrightarrow{BM} \cdot \overrightarrow{BC} = \overrightarrow{MC} \cdot \tau = q_i$$
In which $q_i = \overrightarrow{BC}$ is the motional variation amount of the slider relative to the guide.

Letting $c_i = \overrightarrow{BM} \cdot \tau$, (8) can be re-arranged as:
$$\overrightarrow{BM} \cdot \overrightarrow{BC} = c_i \cdot q_i$$
Putting (7) and (9) into (6) results in:
$$q_i^2 - 2 \cdot c_i \cdot q_i + r_i^2 - L_i^2 = 0$$
Eventually, the two inverse solutions for each motional variation amount of the slider are found explicitly:
$$q_i = c_i \pm \sqrt{c_i^2 - r_i^2 + L_i^2}$$

IV. DERIVATION OF THE JACOBIAN MATRIX

The spherical joints, with the partial freedom, are used in the both ends of the branched chains so that the jaw movement parallel mechanism also has the partial freedom. However, the partial freedom has no impact on the motion performance of the mechanism. Meanwhile, there is no redundancy drive in the mechanism, so the linear relation between each branch chain pose’s input $\theta$ and mandible pose’s output $X$ can be expressed as:
$$f = (\theta, X)$$

Jacobian matrix can be used to describe the relationship between the speed of each branch chain and the mandible platform (the end-effector). According to the (12):
$$f = \begin{bmatrix} \theta \\ \dot{X} \end{bmatrix}$$

According to the Jacobian matrix established by the (13), project the velocity of hinge points $M_i$ and $C_i$ along each branch chain:
$$(\dot{\tau} + \omega \cdot \overrightarrow{OM}_i \cdot \overrightarrow{CM}_i) \cdot \overrightarrow{CM}_i = v_i \tau \cdot \overrightarrow{CM}_i$$
In which $\tau$ and $\omega$ present the translational velocity vector and angular velocity vector, respectively; $v_i$ is the velocity of the slider; $\tau = [0, 0, 1]^T$ is the unit vector direction of the guide. (14) can be rewritten by the matrix form as follows:
$$\begin{bmatrix} \overrightarrow{CM}_1 \\ \overrightarrow{CM}_2 \\ \vdots \\ \overrightarrow{CM}_n \end{bmatrix} = \begin{bmatrix} \overrightarrow{CM}_1 \cdot \tau \\ \overrightarrow{CM}_2 \cdot \tau \\ \vdots \\ \overrightarrow{CM}_n \cdot \tau \end{bmatrix}$$

The matrix form of (15) is:
$$\begin{bmatrix} J_1 \\ J_2 \\ \vdots \\ J_n \end{bmatrix} = \begin{bmatrix} v_1 \\ v_2 \\ \vdots \\ v_n \end{bmatrix}$$
In which, $J_\theta = [\theta_1, \theta_2, ..., \theta_n]^T$.

V. RESEARCH OF SIMULATION EXPERIMENT

A. Establishment of Mandible Simulation Platform and Attitude Definition

First of all, according to the parameters of the mandible platform structure and the muscle insertion points, the paper sets up a virtual prototyping robot model in ADAMS, which can simulate the mandible movement. As shown in figure 4, the simulation of the mandible movement in ADAMS performs 5 periodic motions with interval of 1s and their motion attitude shows as follows: irregular open-closed movement, bite movement, left chew, conventional open-closed movement, and right chew. The difference of the definition between irregular open-closed movement and conventional open-closed movement lies as follows: Irregular open-closed movement can be considered that the mandible performs certain movement in the direction of right and left during the opening and closing movement; Conventional open-closed movement has no such right and left movement. Bite movement means that the mandible not only bites up and down, but also has the action of grind and tore. Left and right chewing movement can be deemed as the process of bite and grind with unilateral tooth.
To analyze the trajectory of the mandible movement, the following reference points are used to describe mandible motion: IP (incisal point), LMP (left first molar point), RMP (right molar point), LCP (left condylar point), RCP (right condylar point). The position of the reference points in mandible coordinate is presented as in TABLE II and Fig.5.

### TABLE II

<table>
<thead>
<tr>
<th>Reference points</th>
<th>X(mm)</th>
<th>Y(mm)</th>
<th>Z(mm)</th>
</tr>
</thead>
<tbody>
<tr>
<td>IP</td>
<td>80.0</td>
<td>0</td>
<td>-38.8</td>
</tr>
<tr>
<td>RMP</td>
<td>45.2</td>
<td>-12.2</td>
<td>2.0</td>
</tr>
<tr>
<td>LMP</td>
<td>45.2</td>
<td>12.2</td>
<td>2.0</td>
</tr>
<tr>
<td>RCP</td>
<td>5.0</td>
<td>-47.3</td>
<td>-5.0</td>
</tr>
<tr>
<td>LCP</td>
<td>5.0</td>
<td>47.3</td>
<td>-5.0</td>
</tr>
</tbody>
</table>

B. *Simulation Experiment of Mandible Platform Movement*

In the cases of five different movement posture defined, considering the symmetry of RCP and LCP as also RMP and LMP, the ADAMS Postprocessor analyzes the reference points IP, RMP, RCP in the X, Y, Z direction of trajectory, as shown in Fig. 6-8 below.

The displacement curves of the three reference points in figures show the relative displacement of the mandible platform from the initial position of the stationary state to the above five kinds of movement.

Through comparisons and analyses, it can be concluded that the relative displacement of IP point in direction Z reaches the largest amount--55.1 mm in 3.5s. At this time the mandible platform is in the stage of the conventional open-closed movement, moreover, the displacement in the direction X of the three reference points is almost zero, which is consistent to human mandible trajectory. In the normal human mandible movement process, the range of mandible upper and lower movement is remarkably large, as also as left and right movement, but the changes are small in the direction of front and back. At 4.5 s, IP point and RCP point in the direction Y have conspicuous mutation, mainly due to the chewing and tearing movement of the mandible platform’s right tooth. In the IP movement situation, for example, the maximum displacement in the direction X, Y and Z are 47.1 mm, 25mm and 55.1mm, respectively, which is consistent with the movement of human incisal point. The fact shows that the jaw movement robot, considering the biomechanical characteristics of the mandible drive muscles and the feasibility of mechanism design, may truly represent human mandible trajectory.

In order to observe the reference points’ trajectory more intuitively, the paper simulates the case of mandible open angle as 30 degrees in Matlab, and analyzes the trajectory of the mandible reference points in three-dimensional space, as shown in Fig.9. The relationship among the reference points movement are: IP > LCP > LMP, which conforms to the position of those reference points in human body. The displacement of IP point in direction X and Z are 25 to 30
mm, which is basically consistent with the movement range of the incisal center point when the opening angle of human mouth is 30 degrees. The result states that the jaw movement robot can meet the reliability requirement of the movement trajectory.

C. Mandible Drive System Analysis

The jaw movement is controlled by the motion of the slider along the guide which is driven by the system consisting of motor and screw-nut, and the branched chains which simulate the closing muscle group drive the mandible platform to realize the human mandible movement trajectory. The posture change of the mandible platform depends on the sliders’ movement range. The figure 10 shows the characteristic curves of the slide movement along the guide in each branched chain.

Figure (a) shows the displacement of the slider, thereupon, it can be concluded that the masseter reaches the maximum displacement at different posture, which is consistent with the characteristics of the masseter in human mandible system. In 4-5 s, the right masseter performs chew movement, whose maximum of the displacement variation is 40 mm, and it can be confirmed that the food is ground manly by the function of masseter at this time. As shown in Fig.(b) and Fig.(c), the velocity and acceleration of the left and right masseters vary alternatively in 1-2 s and 4-5 s periods. The Pterygium has the minimal motional variation during the whole mandible movement process, in that the pterygium is near the axis of the temporomandibular joint in the human mandible system (it can be simply thought that the mandible rotates along the axis). So the pterygium plays an insignificant role in the process of mandible biting movement and hard food chewing. As Fig.(d) shows, with definite load, the changes and sizes of the mandible muscles’ driving force are consistent with the mandible posture at this time. The robot performs the mandible bite movement during 3-4 s, because the load forces and driving forces are in opposite directions, the driving force reaches the largest about 1893 N at the same time. Fig.(e) shows the one side chewing movement in 2-3 s and 4-5s. During the movement, the largest driving power of the temporals is about 144.2 W, which is consistent with the position of the load as well and provides the selection basis of the driving device.

In a word, the simulation experiment shows that this jaw movement robot can truly represent the human mandible movement and the mechanics characteristics.
D. Hardware Configuration and Prototype Model of Mandible Drive System

Under certain load, the jaw movement robot completes such movements as closing, biting and unilateral chewing, so the motors on the drive device should change rotation direction frequently and speed up instantaneously. Considering the gravity of the mandible platform and branched chains, in the process of power up and down, motor brake function should be added to realize the power-off protection, avoiding the sliding of the motors leading to the damage of the mechanism. Meanwhile, as the structure space of the mandible is small, the installing space of the motors should be considered seriously. In a word, in order to meet the motion requirements of the jaw movement robot, including large load, rapid response, and installation requirement, the servomotor which has the advantage of large torque, small moment of inertia, and small volume is chosen. The servomotor parameters of the chewing robot are shown in TABLE III.

As shown in Fig. 11, the prototype of jaw movement robot mainly consists of the static platform I, driving device II, branched chain III, and mandible platform IV. The six branched chains should be assembled in the same way, then collectively connect the static and mandible platforms to complete the robot assembly smoothly.

VI. CONCLUSION

By the mechanical bionic principle, considering the jaw size parameters and jaw driving muscles’ biomechanical characteristics of human mandible system, the paper proposes a new jaw movement robot. Compared with the similar robot, it can reconstruct human mandible movement and mechanics characteristics more accurately. Through the motion performance analysis and simulation experiment research, the paper verifies the feasibility of the structure design, the reliability of the movement trajectory, and the rationality of the bite force, which can lay a foundation for the development of the prototype.

REFERENCES


![Fig.11 Prototype model](image)